

# The Effect of an Acute Bout of Resistance Exercise on Carotid Artery Strain and Strain Rate

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## Abstract

Arterial wall mechanics likely play an integral role in arterial responses to acute physiological stress. Therefore, this study aimed to determine the impact of low and moderate intensity double-leg press exercise on common carotid artery (CCA) wall mechanics using 2D vascular strain imaging. Short-axis CCA ultrasound images were collected in 15 healthy men (age:  $21 \pm 3$  years; stature:  $176.5 \pm 6.2$  cm; body mass;  $80.6 \pm 15.3$  kg) before, during, and immediately after short-duration isometric double-leg press exercise at 30% and 60% of participants' one-repetition maximum (1RM:  $317 \pm 72$  kg). Images were analyzed for peak circumferential strain (PCS), peak systolic and diastolic strain rate (S-SR and D-SR) and arterial diameter. Heart rate (HR), systolic and diastolic blood pressure (SBP and DBP) were simultaneously assessed and arterial stiffness indices were calculated *post hoc*. A two-way repeated measures ANOVA revealed that during isometric contraction, PCS and S-SR decreased significantly ( $P < 0.01$ ) before increasing significantly above resting levels post-exercise ( $P < 0.05$  and  $P < 0.01$  respectively). Conversely, D-SR was unaltered throughout the protocol ( $P = 0.25$ ). No significant differences were observed between the 30% and 60% 1RM trials. Multiple regression analysis highlighted that HR, BP and arterial diameter did not fully explain the total variance in PCS, S-SR and D-SR. Acute double-leg press exercise is therefore associated with similar transient changes in CCA wall mechanics at low and moderate intensities. CCA wall mechanics likely provide additional insight into localized intrinsic vascular wall properties beyond current measures of arterial stiffness.

**Key words:** Circumferential Strain, Strain Rate, Arterial Stiffness, Hemodynamics.

## 1 **Introduction**

2 Arterial responses to acute physiological stress are influenced by sympathetic neural control,  
3 hemodynamic conditions inside the vessel, and arterial wall mechanics. Arterial wall  
4 mechanics refer to the deformation and rate of deformation of an arterial wall in longitudinal,  
5 circumferential and radial planes (15, 31, 42). Due to the progressive change in arterial  
6 structure from large arteries to small arterioles, there is currently no gold standard approach  
7 for the assessment of localized arterial stiffness, which describes the capacity of an artery to  
8 expand and contract in response to pressure changes (2, 3). Furthermore, current techniques  
9 used to measure arterial stiffness such as pulse wave velocity do not permit the examination  
10 of localized arterial wall characteristics, and do not allow for differences between systole and  
11 diastole to be examined. In contrast, novel two-dimensional vascular (2D) strain imaging  
12 quantifies vascular tissue motion during systole and diastole by identifying markers  
13 (speckles) in the traditional grey-scale ultrasound image and subsequently tracking these  
14 throughout the cardiac cycle (2). Peak circumferential strain (deformation), peak systolic  
15 strain rate and peak diastolic strain rate (the rate of deformation during systole and diastole)  
16 are measured directly from the motion of the arterial wall (15, 31, 42). Two-dimensional  
17 vascular strain imaging has previously been validated *in vitro* in the longitudinal, radial and  
18 circumferential planes (18). *In vivo*, common carotid artery (CCA) circumferential strain  
19 imaging has been shown to have the highest feasibility and reproducibility, and is  
20 significantly related to measures of arterial stiffness including  $\beta$  stiffness index, distensibility  
21 coefficient and brachial-ankle pulse-wave velocity (42). The application of this technique  
22 may therefore reveal valuable and novel insight into CCA wall mechanics at rest and during  
23 physiological stress in different populations. For example, this technique has previously been  
24 shown to differentiate arterial wall mechanics between young (< 30 years) and older adults (>  
25 50 years) (2). In older adults, degeneration of elastic fibers and compensatory increases in

26 arterial wall collagen are known to occur (31). In the study of Bjällmark *et al.*, this was  
27 reflected in significant reductions in resting CCA peak circumferential strain (PCS), as well  
28 as peak systolic and diastolic strain rates (S-SR and D-SR respectively) in the older adults  
29 compared to the younger adults (2). The authors suggest that a higher strain rate is beneficial  
30 as this may be indicative of a greater arterial elasticity (2). It is therefore possible that the use  
31 of circumferential strain imaging to assess arterial wall mechanics might complement  
32 existing measures of arterial stiffness by providing a sensitive, non-invasive method to  
33 examine the localized intrinsic properties of the arterial wall between populations, at rest and  
34 during physiological stress.

35

36 During acute resistance exercise, arteries are exposed to numerous stimuli including  
37 increased blood flow (13), shear stress (11), and blood pressure (12, 24), as well as  
38 mechanical compression as a result of muscular contraction (23). These responses have been  
39 shown to occur locally in the artery of the exercising limb (10, 11) as well as remotely in  
40 arteries located in non-exercising tissues (36, 37). CCA arterial stiffness is also known to  
41 increase following an acute bout of resistance exercise (21). Despite this, and the well-known  
42 impact of acute resistance exercise on arterial hemodynamics, the effect of an acute bout of  
43 resistance exercise on CCA wall mechanics is not known. An understanding of how arterial  
44 wall mechanics change *during* an acute bout of resistance exercise, when blood pressure is  
45 significantly elevated, might provide insight into the mechanisms responsible for the increase  
46 in arterial stiffness previously reported (21). This is of particular importance in the CCA, as  
47 the brain is extremely susceptible to hemodynamic pulsatility (14, 28) and a reduction in the  
48 ability to buffer elevations in both blood pressure and flow have been associated with an  
49 increased risk of stroke (25, 41). Investigation of CCA wall mechanics during resistance  
50 exercise might also provide further insight into the specific mechanisms that underpin

51 training-induced vascular remodeling of the CCA, characterized by a decreased wall  
52 thickness (32) and increased diameter (33).

53

54 Based on the above considerations, the primary aim of this study was to examine changes in  
55 PCS, S-SR and D-SR in the CCA during an acute bout of double-leg press exercise.  
56 Consequential to the significant increase in heart rate (HR), blood pressure and arterial  
57 diameter, it was hypothesized that PCS, S-SR and D-SR would decrease significantly during  
58 the double-leg press, before returning to baseline immediately post-exercise. It was also  
59 hypothesized that more pronounced changes would occur during moderate versus low  
60 intensity exercise. A secondary aim of the study was to investigate whether CCA PCS, S-SR  
61 and D-SR at rest, during isometric contraction, and immediately post-exercise are dependent  
62 on HR, blood pressure and CCA diameter. It was hypothesized that HR, blood pressure and  
63 CCA diameter would only partly explain PCS, S-SR and D-SR and as such, these novel  
64 parameters could partially reflect acute alterations to the localized intrinsic properties of the  
65 CCA wall during physiological stress.

66

## 67 **Methods**

### 68 *Participants*

69 A total of 15 healthy recreationally active men (age:  $21 \pm 3$  years; stature:  $176.5 \pm 6.2$  cm;  
70 mass;  $80.6 \pm 15.3$  kg; leg-press 1RM:  $317 \pm 72$  kg) volunteered to participate and provided  
71 written informed consent prior to testing. All participants were non-smokers, normotensive,  
72 had no previous history of cardiovascular, musculoskeletal or metabolic disease, and were not  
73 taking any prescribed medication. The study protocol was approved by the Cardiff  
74 Metropolitan University School of Sport Research Ethics Committee, and adhered to the  
75 Declaration of Helsinki (2008).

76

77 *Experimental Procedures*

78 Participants reported to the laboratory on two separate occasions and were asked to refrain  
79 from strenuous exercise, alcohol and caffeine intake for 24 hours prior to each visit. During  
80 the first visit, the participants' 1 repetition maximum (1RM) was determined for the double-  
81 leg press exercise in accordance with guidelines set by the National Strength and Conditional  
82 Association (1), without the use of a Valsalva maneuver. During the second visit,  
83 participants' body mass and stature were recorded and a standardized warm up protocol was  
84 completed consisting of one set of ten repetitions at both 10% 1RM and 20% 1RM with a  
85 two-minute rest period between each set. Participants were then seated on the leg-press  
86 machine where they rested for 5 minutes, whilst a cuff was attached to the middle phalanx of  
87 the middle finger of the right hand for continuous beat-by-beat measurement of BP  
88 (FinometerPro, FMS, Amsterdam, Netherlands), and HR was recorded via ECG (Vividq, GE  
89 Medical Systems Israel LTD). A single trained sonographer collected 2D grey-scale images  
90 of the CCA short-axis 1) before, 2) during isometric contraction, and 3) immediately (~12  
91 seconds) after double-leg press exercise equal to 30% and 60% of 1 RM. At both exercise  
92 intensities two repetitions were completed, each beginning with a dynamic leg extension.  
93 Subsequently each participant was instructed to simultaneously lower the double-leg press to  
94 a predetermined, standardized position (knee flexion angle of 90°), whilst exhaling to natural  
95 end-expiration (functional residual capacity). The participant was then verbally instructed to  
96 hold this position (~5 seconds) for image acquisition during isometric effort, before repeating  
97 the dynamic leg extension to complete the repetition. Simultaneous collection of all vascular  
98 and hemodynamic measurements ensured that variables were time aligned throughout the  
99 protocol. The order of intensity was randomized and counterbalanced throughout the  
100 experiment. Images were collected using a commercially available ultrasound system with a

101 12 MHz linear array transducer (Vividq, GE Medical Systems Israel LTD) and all exercise  
102 was performed on a commercially available leg-press machine (Linear Leg Press, Life  
103 Fitness (UK) Ltd, Queen Adelaide, UK).

104

#### 105 *Vascular Ultrasonography and 2D-Strain Imaging*

106 Two-dimensional short-axis grey-scale cine loops of the CCA were recorded 1-2 cm below  
107 the carotid bulb over a minimum of three consecutive cardiac cycles, and stored for  
108 subsequent offline analysis using dedicated 2D-strain software (EchoPac Version 112, GE  
109 Vingmed Ultrasound, Horten Norway). Two-dimensional strain software quantifies vascular  
110 tissue motion by automatically identifying speckles in the ultrasound image, which are  
111 subsequently tracked across the cardiac cycle (2). PCS of the CCA (which reflects the  
112 circumferential deformation of the arterial wall from diastole to peak systole), peak S-SR and  
113 D-SR (which reflect the maximal rate of circumferential deformation during systole and  
114 diastole respectively) were determined by manually placing a region of interest (ROI) over  
115 the cross-sectional area of the CCA, and subsequently adjusting the ROI to ensure accurate  
116 alignment with the arterial wall. Within this ROI, movement of the speckles were tracked  
117 frame by frame throughout systole and diastole using a speckle tracking algorithm inherent to  
118 the software (Figure 1), which resulted in the production of strain and strain rate curves  
119 (Figures 2A and 2B, respectively). Adequate tracking of the CCA was objectively verified  
120 according to a quality assurance tool inherent to the software, and also visually confirmed by  
121 the operator, who manually adjusted the ROI, if necessary. All offline analyses were  
122 completed by a single operator. PCS, S-SR and D-SR, were measured as an average over the  
123 circumference of the CCA (the entire ROI), providing 'global' values for each of the  
124 variables. As previously defined (31), PCS was identified as the greatest peak in the  
125 circumferential strain curve (Figure 2A), peak S-SR was identified as the first positive peak in

126 the strain rate curve which occurred after the QRS complex, and peak D-SR was determined  
 127 as the first negative peak in the strain rate curve which occurred after the T-wave of the ECG  
 128 (Figure 2B). All 2D-strain measurements were averaged for three consecutive beats. Peak  
 129 systolic and peak diastolic CCA diameters ( $Diam_{SYS}$  and  $Diam_{DIAS}$  respectively) were defined  
 130 as the maximum and minimum diameters during the cardiac cycle. Arterial diameter was  
 131 measured manually using calipers from the leading edge of the intima-lumen interface of the  
 132 anterior wall to the leading edge of the lumen-intima interface of the posterior wall of the  
 133 short-axis image (30, 31), thus ensuring that all CCA parameters (PCS, S-SR, D-SR,  $Diam_{SYS}$   
 134 and  $Diam_{DIAS}$ ) were measured from the same image.

135

136 To determine changes in stiffness of the CCA throughout the double-leg press exercise,  
 137 Peterson's elastic modulus ( $E_p$ )  $\beta_1$  stiffness index and  $\beta_2$  stiffness index were calculated as  
 138 follows:

$$139 \quad E_p = (SBP - DBP) / ((Diam_{SYS} - Diam_{DIAS}) / Diam_{DIAS}) \quad \text{in kPa} \quad (1)$$

$$140 \quad \beta_1 = \ln (SBP / DBP) / ((Diam_{SYS} - Diam_{DIAS}) / Diam_{DIAS}) \quad \text{in cm}^2/\text{kPa} \quad (2)$$

$$141 \quad \beta_2 = \ln (SBP - DBP / PCS) \quad (3)$$

142 where SBP and DBP are systolic and diastolic blood pressures respectively and  $\ln$  refers to  
 143 the natural logarithm function.  $E_p$  and  $\beta_1$  are conventional measures of arterial stiffness and  
 144 adjust changes in arterial diameter throughout the cardiac cycle for changes in distending  
 145 pressure (19).  $\beta_2$  incorporates measured peak circumferential strain and relates this to  
 146 distending pulse pressure (30, 31). An increase in  $E_p$ ,  $\beta_1$  and  $\beta_2$  stiffness indices is indicative  
 147 of a greater arterial stiffness compared with baseline in this particular anatomical region, at a  
 148 given point in time.

149

## 150 *Statistical Analysis*

151 The reproducibility of PCS, S-SR and D-SR was assessed prior to the experimental protocol  
152 and the intra-observer variability was determined by calculating coefficients of variation  
153 (CV). Normality of experimental data was examined and confirmed using the Shapiro-Wilk  
154 test. A two-way repeated measures ANOVA was used to identify differences in all variables  
155 between the three phases of the movement (pre lift, during isometric contraction, post lift)  
156 and exercise intensity (30% and 60% of 1 RM), followed by paired samples *t* tests to identify  
157 differences. Standard multiple regression analysis was used to determine whether CCA PCS,  
158 S-SR and D-SR at rest, during and immediately post-exercise were dependent on HR, SBP,  
159 DBP, Diam<sub>SYS</sub> or Diam<sub>DIAS</sub>. For all statistical analysis, SPSS version 19.0 (Chicago, IL) was  
160 used and significance was accepted at 0.05. Data are presented as means  $\pm$  SD.

161

## 162 **Results**

### 163 *Heart rate, blood pressure and common carotid arterial diameter*

164 During isometric contraction at both intensities, HR, SBP, DBP, Diam<sub>SYS</sub> and Diam<sub>DIAS</sub>  
165 increased significantly from baseline levels (all  $P < 0.01$ , Figure 3). Following exercise SBP,  
166 Diam<sub>SYS</sub> and Diam<sub>DIAS</sub> returned to baseline, whereas DBP dropped significantly below  
167 previous baseline levels ( $P < 0.01$ ). In contrast, HR decreased significantly after the double-leg  
168 press ( $P < 0.01$ ), but remained significantly elevated following exercise in comparison to  
169 baseline ( $P < 0.01$ ). There were no statistically significant differences between the 30% and  
170 60% 1RM exercise intensities for any of the parameters examined ( $P > 0.05$ ).

171

### 172 *Arterial wall mechanics*

173 During isometric contraction, PCS decreased from baseline at both 30% 1RM and 60% 1RM.  
174 The decrease in PCS was accompanied by a significant decrease in S-SR at both 30% 1RM  
175 and 60% 1RM. Immediately post-exercise, PCS and S-SR increased significantly above  
176 baseline. In contrast, D-SR remained unaltered throughout the experimental procedure  
177 ( $P=0.25$ , Figure 3B). Again, no statistically significant differences were detected between the  
178 30% and 60% 1RM exercise trials for any of the arterial variables examined ( $P>0.05$ ).

179

### 180 *Stiffness parameters*

181 During isometric contraction  $E_p$ , as well as  $\beta_1$  and  $\beta_2$  stiffness indexes increased significantly  
182 from baseline ( $P<0.01$ , Table 1). Immediately post-exercise, all three stiffness parameters  
183 returned to baseline. No statistically significant differences were identified between the 30%  
184 and 60% 1RM exercise trials for any of the arterial stiffness variables examined ( $P>0.05$ ).

185

### 186 *Determinants of arterial wall mechanics*

187 Multiple regression analysis showed that collectively, HR, SBP, DBP, Diam<sub>SYS</sub>, and  
188 Diam<sub>DIAS</sub> explained between 14 - 81% of the total variance in PCS, S-SR and D-SR at rest,  
189 27 - 66% during isometric contraction and 39 - 53% immediately post exercise (Table 2).  
190 The regression analysis also highlighted significant individual predictor variables for PCS, S-  
191 SR and D-SR at rest, during isometric contraction and immediately post-exercise, which are  
192 described below.

193

### 194 *Peak circumferential strain*

195 At rest, Diam<sub>SYS</sub>, and Diam<sub>DIAS</sub> were identified as significant predictors of PCS ( $\beta=1.78$ ,  
196  $P<0.01$  and  $\beta=-1.97$ ,  $P<0.01$  respectively). In contrast, HR and SBP were identified as  
197 significant individual predictors for PCS during exercise ( $\beta= -0.72$ ,  $P<0.05$ , and  $\beta= -0.38$ ,

198  $P < 0.05$  respectively), whereas HR and DBP were identified as significant individual  
199 predictors of PCS immediately post exercise ( $\beta = 0.48$ ,  $P < 0.05$ , and  $\beta = -0.70$ ,  $P < 0.05$   
200 respectively).

201

#### 202 *Systolic strain rate*

203 As with PCS,  $\text{Diam}_{\text{SYS}}$ , and  $\text{Diam}_{\text{DIAS}}$  were identified as significant individual predictors of S-  
204 SR at rest ( $\beta = 1.18$ ,  $P < 0.01$  and  $\beta = -1.08$ ,  $P < 0.01$  respectively). No significant individual  
205 predictors were identified for S-SR during isometric contraction, whereas HR and DBP were  
206 identified as significant individual predictors of S-SR immediately post-exercise ( $\beta = 0.60$ ,  
207  $P < 0.01$ , and  $\beta = -0.58$ ,  $P < 0.05$  respectively).

208

#### 209 *Diastolic strain rate*

210 No significant individual predictors were identified for D-SR at rest or during exercise  
211 however, HR was identified as significant individual predictor of D-SR immediately post-  
212 exercise ( $\beta = -0.48$ ,  $P < 0.01$ ).

213

#### 214 ***Reproducibility of measurements***

215 The reproducibility of measurements of 2D strain imaging parameters was assessed in our  
216 laboratory. The CV for the intra-observer reliability of CCA PCS was 2.3%, which is  
217 considerably lower than the 3.9%, 5.8% and 8.8% previously reported in the literature (2, 4,  
218 42). The CV for the intra-observer reliability of S-SR and D-SR was 5.4% and 6.0%  
219 respectively, which is in agreement with previously reported values (2). The CV for the intra-  
220 observer reliability of  $E_p$  and  $\beta_1$  was 29% and 25% respectively, which is higher than the 18%  
221 previously reported (2). The CV for the intra-observer reliability of  $\beta_2$  was 18%. In

222 accordance with previous research, the variability of the stiffness parameters ( $E_p$ ,  $\beta_1$  and  $\beta_2$ )  
223 was considerably higher than that of PCS, S-SR and D-SR (2).

224

## 225 **Discussion**

226 The aims of this study were to investigate changes in PCS, S-SR and D-SR of the CCA in  
227 response to an acute bout of double-leg press exercise and to examine whether PCS, S-SR  
228 and D-SR at rest, during isometric contraction and immediately post-exercise were dependent  
229 on heart rate (HR), blood pressure and CCA diameter. The novel findings of the present study  
230 were twofold: (i) an acute bout of double-leg press exercise causes significant changes in  
231 CCA PCS and S-SR but not D-SR, during isometric contraction and immediately post-  
232 exercise, and (ii) HR, SBP, DBP,  $Diam_{SYS}$  and  $Diam_{DIAS}$  only partly explain the total  
233 variance in PCS, S-SR and D-SR at rest, during isometric contraction, and immediately  
234 following an acute bout of double-leg press exercise.

235

### 236 *Acute resistance exercise and common carotid arterial wall mechanics*

237 Despite no change in D-SR throughout the exercise protocol, PCS and S-SR decreased  
238 significantly during isometric contraction; a finding which provides support for acute changes  
239 in systolic arterial wall mechanics in vessels located in non-exercising tissues. As  
240 hypothesized, PCS and S-SR (but not D-SR) decreased significantly during isometric  
241 resistance exercise, and standard multiple regression revealed that this was partly explained  
242 by HR, blood pressure and arterial diameter. Measurements obtained immediately after  
243 exercise showed that PCS significantly increased, exceeding baseline levels and this was  
244 accompanied by a significant increase in S-SR, despite  $Diam_{SYS}$  and SBP returning to  
245 baseline. As previously suggested, it is possible that the increase in PCS and S-SR observed

246 immediately post-exercise may indicate a greater arterial elasticity, as a result of acute  
247 changes to the intrinsic properties of the CCA wall (2). The increase in S-SR immediately  
248 post-exercise may occur to buffer the elevated blood pressure associated with the onset of  
249 exercise, providing a smoother, more consistent flow (17) and preventing damage to cerebral  
250 microvessels (29). The post-exercise changes in both PCS and S-SR shown in the present  
251 study may also represent important stimuli for the chronic vascular remodeling observed  
252 following resistance training. Increased distension of the arterial wall has previously been  
253 shown to result in greater stretching of the load-bearing lamellae, augmenting arterial wall  
254 stress (20). Indeed, cyclic strain has been identified as a major determinant of the phenotype  
255 of vascular smooth muscle cells (VSMCs) *in vitro* (20). Cyclic stretching has previously been  
256 shown to exert a greater influence on growth of the VSMCs than a static load, particularly in  
257 elastic arteries such as the CCA, where greater fluctuations in diameter occur throughout the  
258 cardiac cycle (20). Despite there being no differences in post-exercise arterial stiffness  
259 indices compared to baseline, the results of this study suggest that a bout of double-leg press  
260 exercise causes acute increases in CCA wall deformation and the rate of deformation during  
261 systole, as evidenced by the significant increase in PCS and S-SR immediately post-exercise.  
262 Increased deformation of the CCA after an acute bout of resistance exercise may therefore  
263 represent the primary stimulus for the vascular remodeling associated with resistance training  
264 (31, 32). However, further research is needed to support this hypothesis.

265

266 The lack of differences in calculated arterial stiffness indices immediately post-exercise helps  
267 to illustrate that 2D vascular strain imaging might be a more sensitive measure to accurately  
268 detect changes in localized arterial wall function following acute physiological stress. This  
269 technique may complement existing measures of arterial stiffness by providing additional  
270 insight into localized intrinsic vascular wall properties beyond current established measures.

271

272 ***Determinants of arterial wall mechanics***

273 As hypothesized, the multiple regression analysis revealed that HR, SBP, DBP, Diam<sub>SYS</sub> and  
274 Diam<sub>DIAS</sub> did not fully explain the total variance in PCS, S-SR and D-SR at rest, during  
275 isometric contraction or immediately post-exercise. Resting PCS, for example, was largely  
276 explained by HR, blood pressure and arterial diameter, whereas 61% of the total variance in  
277 S-SR immediately post-exercise was unexplained, despite both HR and DBP being identified  
278 as significant independent predictor variables. Similarly, between 52 - 86% of the total  
279 variance in D-SR was not explained by HR, blood pressure or arterial diameter. Therefore,  
280 although speculative, we suggest that some of the unexplained variance in arterial wall  
281 mechanics observed in the present study might be attributed to acute intrinsic alterations of  
282 the vascular wall in response to physiological stress. It is thought that less than 10% of  
283 collagen fibers are engaged at rest, however at higher pressures, such as during double-leg  
284 press exercise, collagen fibers support wall tension, increasing arterial stiffness to prevent  
285 overstretching and subsequent rupture of the arterial wall (38). In support, an increase in  
286 arterial stiffness during isometric contraction (as evidenced by a rise in the stiffness indices  
287 calculated *post hoc*) was observed in the present study. In contrast to previous research, this  
288 increase in arterial stiffness was transient and present only *during* isometric exercise (21). A  
289 shift towards stiffer collagen fibers, accompanied by an increase in HR and arterial diameter  
290 might therefore explain the reduction in PCS and S-SR observed during isometric  
291 contraction. Immediately post-exercise, the CCA becomes more distensible as arterial  
292 diameter and SBP return to baseline, and elastin rather than collagen, is primarily responsible  
293 for the transfer of stress through the CCA wall (38). These changes, accompanied by an  
294 increase in pulse pressure and an elevation of HR, could account for the significant increases  
295 in PCS and S-SR immediately post-exercise.

296

297 In contrast to PCS and S-SR, there was no significant change in CCA D-SR throughout the  
298 exercise protocol, despite significant increases in diastolic arterial diameter and pressure  
299 during isometric contraction (Figure 3B). This implies that CCA D-SR is not influenced by  
300 resistance exercise-induced changes in arterial diameter or pressure. In support, multiple  
301 regression analysis also highlighted that D-SR was the parameter least influenced by HR,  
302 blood pressure and arterial diameter both at rest and during isometric contraction. Previously,  
303 significant reductions in resting CCA D-SR have been observed in older adults where  
304 degeneration of elastic fibers and compensatory increases in arterial wall collagen are known  
305 to occur (2). Based on the results of the present study, we therefore propose that D-SR might  
306 be an important parameter to accurately reflect changes in the localized intrinsic properties of  
307 the arterial wall, independent of heart rate, blood pressure and arterial diameter. In the future,  
308 examination of CCA D-SR in elderly and clinical populations where changes in the  
309 composition of arterial wall collagen and elastin have occurred could provide support for this  
310 hypothesis. Additionally, further research is needed to determine the true independent  
311 individual influence of other physiological variables such as HR, stroke volume (SV), arterial  
312 diameter, blood pressure, pulse pressure and mean arterial pressure on acute changes in  
313 arterial wall mechanics. Identification of the most influential physiological variables may  
314 allow for CCA PCS, S-SR and D-SR to be normalized appropriately to the loading stimuli. In  
315 the present study, no single physiological variable was identified as a significant predictor for  
316 CCA PCS, S-SR and D-SR, and therefore normalization of these variables was not possible.

317

318 *Acute resistance exercise and arterial hemodynamics*

319 As expected, and in accordance with previous research, a significant rise in HR, SBP and  
320 DBP was observed during double-leg press exercise (12, 24, 26). Immediately post-exercise,  
321 SBP returned to baseline, whereas a significant drop in DBP below baseline levels was  
322 observed. The decrease in DBP might be attributed to a reduction in both the force of muscle  
323 contraction and intramuscular pressure on cessation of exercise. In contrast to previous  
324 research and our initial hypothesis, acute changes in arterial hemodynamics did not differ  
325 between exercise intensities (9, 16, 39). This may however, be explained by the small number  
326 of repetitions, as previous research has highlighted that a single repetition at 100% 1RM  
327 elicits less hemodynamic changes than a higher number of repetitions at a lower intensity  
328 (40).

329

### 330 *Acute resistance exercise and common carotid arterial diameter*

331 Previous research investigating the influence of acute resistance exercise on CCA diameter  
332 have only reported values at rest and immediately post-exercise (5, 21). Results of the  
333 present study indicate that, irrespective of exercise intensity (30% and 60% 1RM), both  
334  $Diam_{SYS}$  and  $Diam_{DIAS}$  increased significantly *during* isometric resistance exercise, before  
335 returning to baseline immediately post exercise. CCA smooth muscle is known to be  
336 innervated by sympathetic efferents (35) and significant increases in vasoconstrictor  
337 sympathetic nerve activity are known to occur during isometric exercise, even at low  
338 intensities (7). In contrast to this,  $Diam_{SYS}$  and  $Diam_{DIAS}$  increased during isometric exercise  
339 in our trial, suggesting that distending forces supersede smooth muscle contraction (35). This  
340 increase in CCA diameter during isometric resistance exercise is unlikely to have occurred as  
341 a result of an increase in SV, as previous research has consistently reported that SV remains  
342 unchanged or decreases during an acute bout of resistance exercise (6, 22, 27). Whilst not

343 measured during the present study, published data from our laboratory has previously  
344 reported a decrease in SV during double-leg press exercise, using a similar protocol (34),  
345 attributed to a combination of decreased preload and increased afterload (22). The transient  
346 increase in CCA diameter observed in the present study is likely related to the significant  
347 increase in blood pressure which has consistently been shown to occur during resistance  
348 exercise (12, 24). In support, a significant relationship between changes in CCA mean  
349 diameter and pressure has previously been shown during strenuous dynamic exercise (35).

350

### 351 *Limitations*

352 The lack of data available on the acute cardiovascular responses to resistance exercise has  
353 previously been attributed to difficulties associated with accurate determination of vascular  
354 assessment during resistance exercise (8). To overcome this issue, images were collected  
355 during a brief isometric hold and whilst this lacks ecological validity, it does allow accurate  
356 data to be collected. Stiffness indices were calculated to relate the changes in arterial pressure  
357 and diameter however, as blood pressure and arterial lumen diameter were measured in the  
358 brachial and carotid arteries respectively, this could have resulted in an overestimation of  
359 arterial stiffness and must therefore be recognized as a limitation. We were unable to measure  
360 SV during the present study and are therefore unable to draw firm conclusions about the  
361 interaction between cardiac and vascular responses to an acute bout of resistance exercise. In  
362 the future, simultaneous measurements of cardiac and vascular responses would be  
363 informative in developing a greater understanding of the acute cardiovascular responses to  
364 resistance exercise. Vascular responses to an acute bout of resistance exercise should also be  
365 measured in other arteries, both central and peripheral, to understand how responses differ in  
366 elastic and muscular arteries. Acute vascular responses during high intensity resistance  
367 exercise and the influence of training status should also be considered. Despite these

368 limitations, 2D vascular strain imaging is a simple technique, which can provide additional  
369 insight into the mechanical behavior of the arterial wall, allowing for differences between  
370 systole and diastole to be examined, and regional comparisons to be made between arteries.  
371 Whilst this technique is not likely to replace established and validated measures of arterial  
372 stiffness, it could complement existing measures and provide further insight into localized  
373 arterial wall function throughout the cardiac cycle, both within and between different  
374 populations.

375

## 376 **Conclusion**

377 Using novel 2D vascular strain imaging, this study has shown that acute changes in systolic  
378 (PCS and S-SR), but not diastolic (D-SR) arterial wall mechanics occur in the CCA *during*  
379 and immediately post an acute bout of double-leg press exercise, at both low and moderate  
380 intensities. The systolic responses may indicate greater elasticity of the CCA immediately  
381 post-exercise, or reflect a protective mechanism to buffer the elevated blood pressure  
382 associated with the onset of resistance exercise, preventing damage to cerebral microvessels.  
383 In contrast, CCA D-SR is not influenced by significant changes in arterial diameter or  
384 pressure during isometric resistance exercise and may therefore be an important parameter to  
385 accurately reflect changes in localized intrinsic vascular wall properties, although further  
386 research is still required.

387

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393

394 **Conflicts of Interest**

395 There is no funding to be declared in relation to this study and the authors have no conflict of  
396 interest.

397

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**Figure 1.** A region of interest placed over a cross-sectional short-axis image of the CCA.

**Figure 2.** (A) Example of a circumferential strain curve produced following speckle tracking of the CCA and; (B) Example of a circumferential strain rate curve produced following speckle tracking of the CCA; Global measurements are represented by white, dotted lines; PCS, peak S-SR and peak D-SR are labeled using white arrows.

**Figure 3.** (A) Systolic parameters ( $Diam_{SYS}$ , SBP and S-SR), (B) diastolic parameters ( $Diam_{DIAS}$ , DBP and D-SR), and (C) HR, mean arterial pressure (MAP) and PCS of the common carotid artery (CCA), at rest, during and after double-leg press exercise at 30% and 60% of 1RM (white and black squares, respectively). \*:  $P < 0.05$  vs. pre; †:  $P < 0.05$  vs. during; values are means  $\pm$  SD.

**Table 1.** Stiffness parameters at rest, during and immediately following double-leg press exercise at 30% and 60% of 1RM.

Variable	30% 1RM			60% 1RM		
	Rest	During	Post	Rest	During	Post
$E_p$ (kPa)	43.5 ± 11.7	88.4 ± 29.6*	43.8 ± 11.8†	47.6 ± 15.2	80.7 ± 24.3*	46.3 ± 14.9†
$\beta_1$ stiffness index (mm <sup>2</sup> /kPa)	3.0 ± 0.7	4.9 ± 1.5*	3.2 ± 0.7†	3.3 ± 0.8	4.3 ± 1.1*	3.3 ± 0.8†
$\beta_2$ stiffness index	1.7 ± 0.3	2.4 ± 0.5*	1.7 ± 0.3†	1.8 ± 0.3	2.3 ± 0.4*	1.7 ± 0.3†

$E_p$ : Peterson's elastic modulus; \*  $P < 0.05$  vs. pre; †  $P < 0.05$  vs. during; values are means ± SD.

**Table 2.** Percentage of the total variance in arterial wall mechanics explained by the combination of HR, SBP, DBP, Diam<sub>SYS</sub>, and Diam<sub>DIAS</sub> at rest, during isometric contraction, and immediately following double-leg press exercise.

Variable	Time	Total Variance Explained (%)	Effect size ( $f^2$ )	P-Value	Significant predictor variables
PCS	Pre	81	4.26	< 0.01	Diam <sub>SYS</sub> , and Diam <sub>DIAS</sub>
	During	66	1.94	< 0.01	HR and SBP
	Post	53	1.13	< 0.01	HR and DBP
S-SR	Pre	65	1.86	< 0.01	Diam <sub>SYS</sub> , and Diam <sub>DIAS</sub>
	During	48	0.92	< 0.05	-
	Post	39	0.64	< 0.05	HR and DBP
D-SR	Pre	14	0.16	0.62	-
	During	27	0.37	0.33	-
	Post	48	0.92	< 0.01	HR

PCS: peak circumferential strain; S-SR: systolic strain rate; D-SR: diastolic strain rate. Significant individual predictor variables for PCS, S-SR and D-SR at rest, during and immediately post-exercise are discussed in the text.